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Griffith

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(54) **COCHLEAR IMPLANT SYSTEMS
INCLUDING MAGNETIC FLUX
REDIRECTION MEANS**

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2009, now Pat. No. 8,897,883.

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A61N 1/37 (2006.01)
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None
See application file for complete search history.

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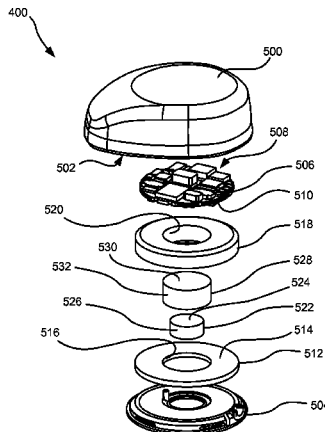
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(57) **ABSTRACT**

An exemplary cochlear implant system includes a component
that houses a circuit board comprising electronic circuitry
that generates one or more signals, an induction coil that
transmits the one or more signals by generating a telemetry
magnetic field, and a telemetry flux guide positioned between
and in direct contact with a top surface of the induction coil
and a bottom surface of the circuit board.

20 Claims, 7 Drawing Sheets



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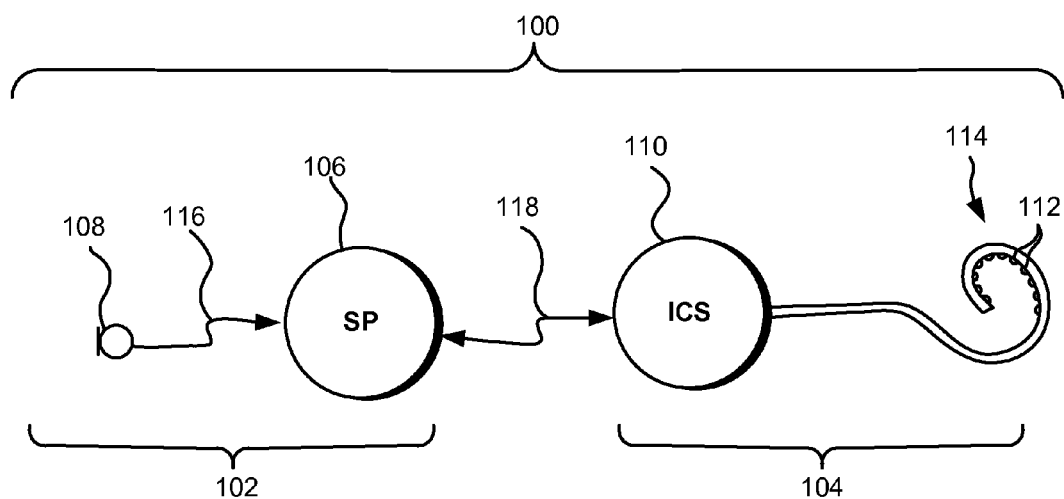


Fig. 1A

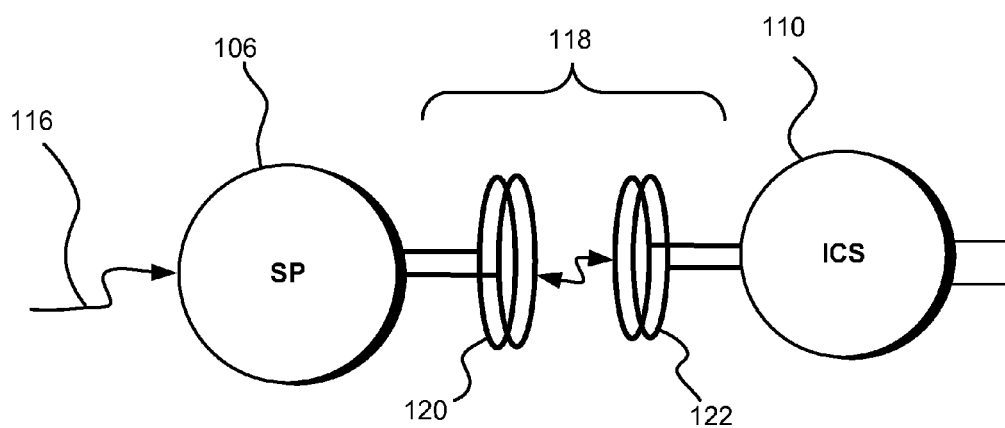


Fig. 1B

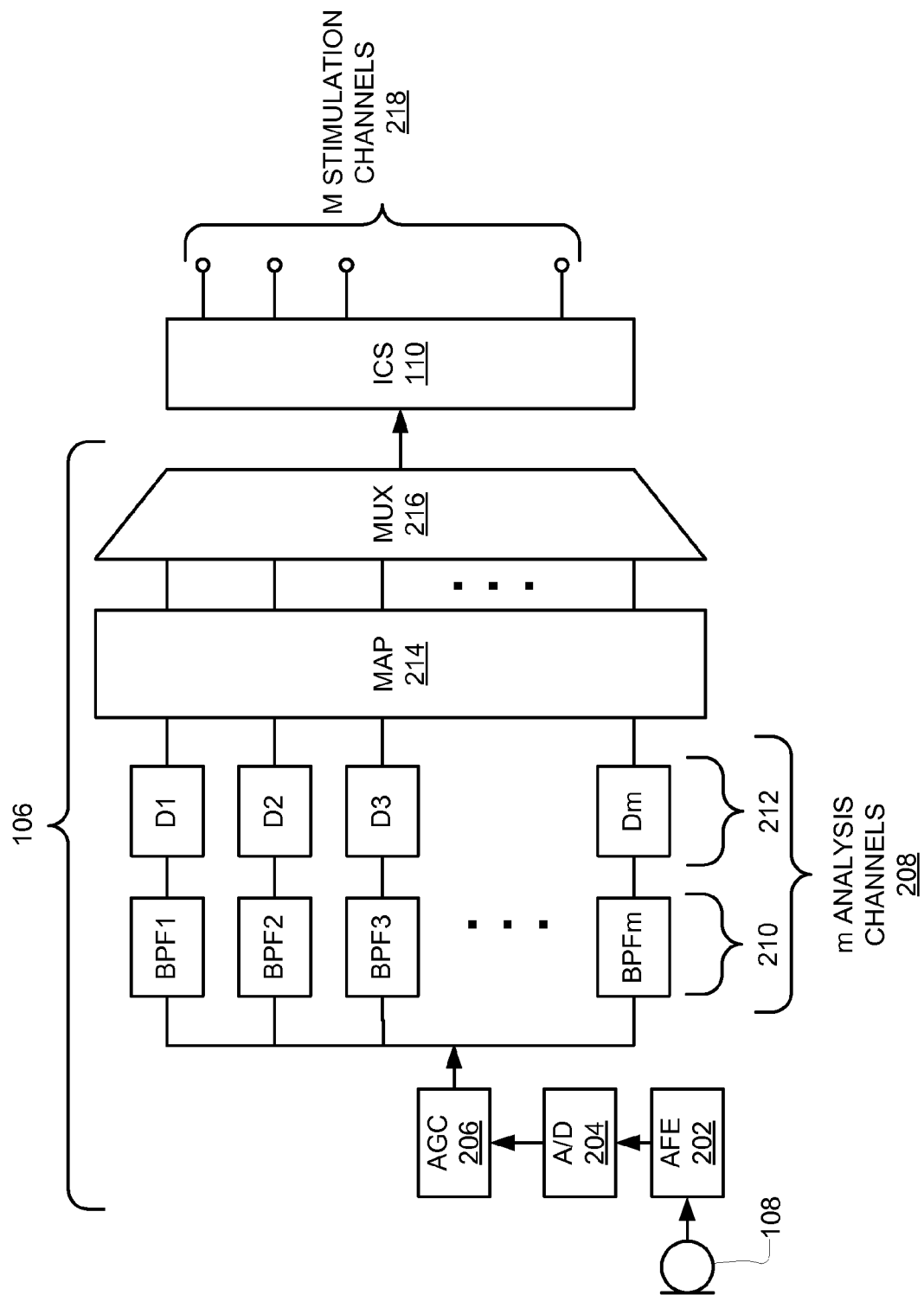
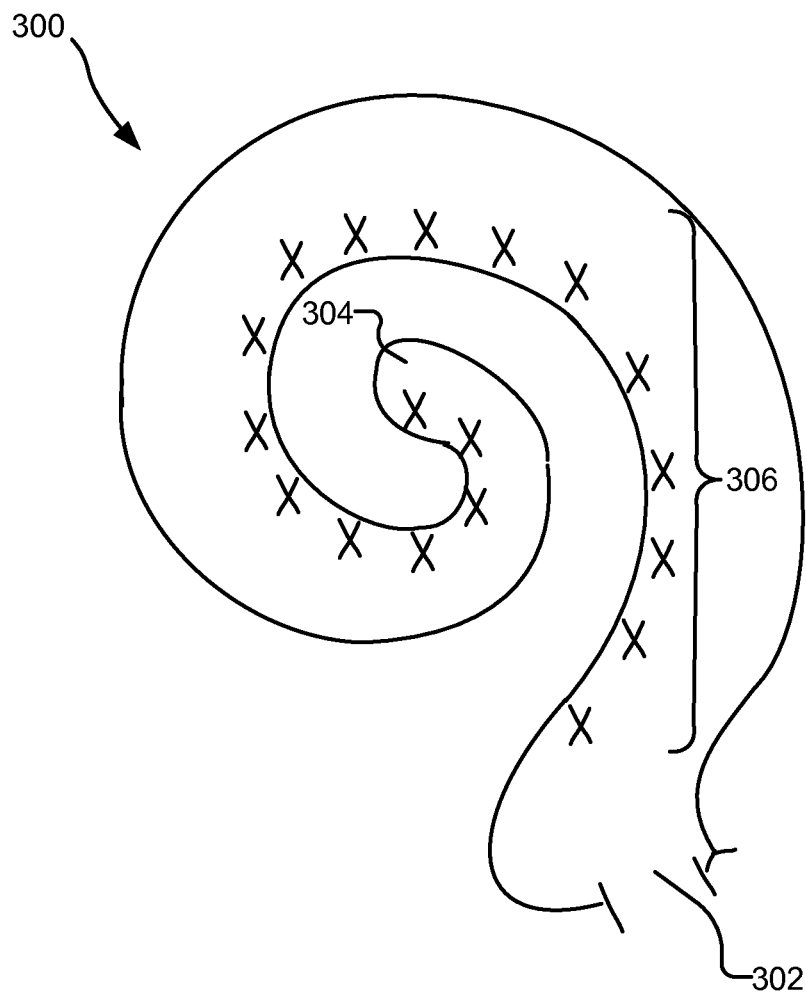


Fig. 2

**Fig. 3**

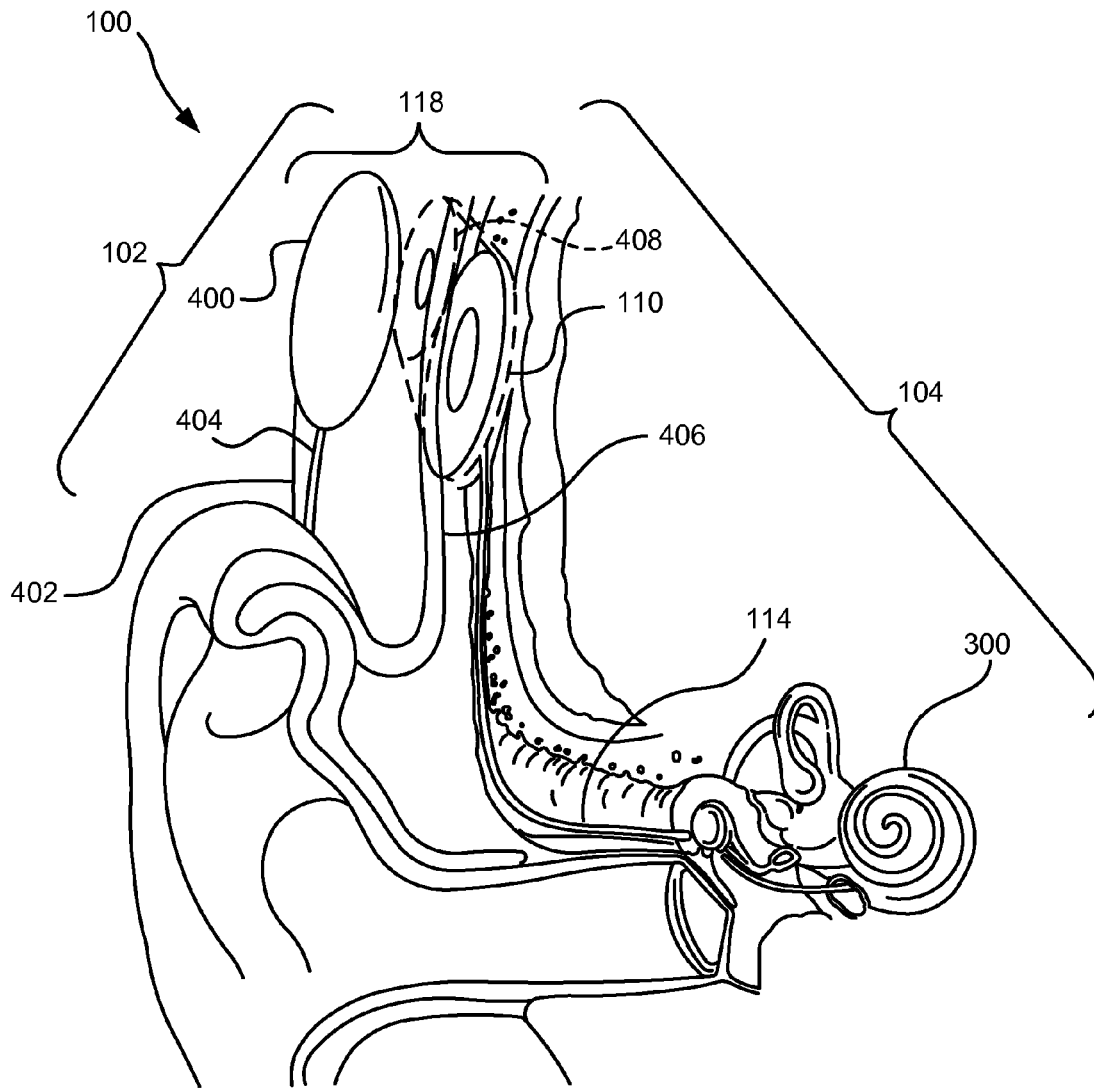


Fig. 4

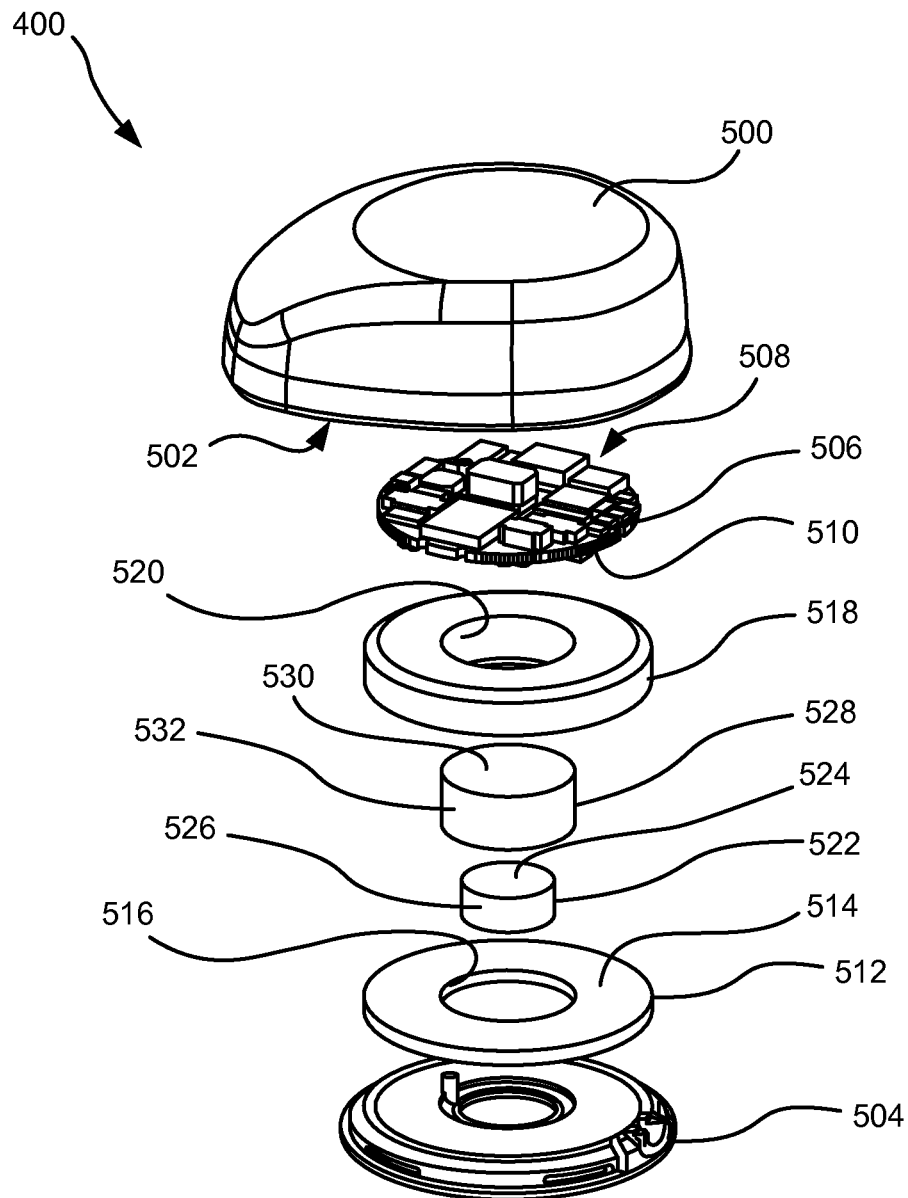


Fig. 5A

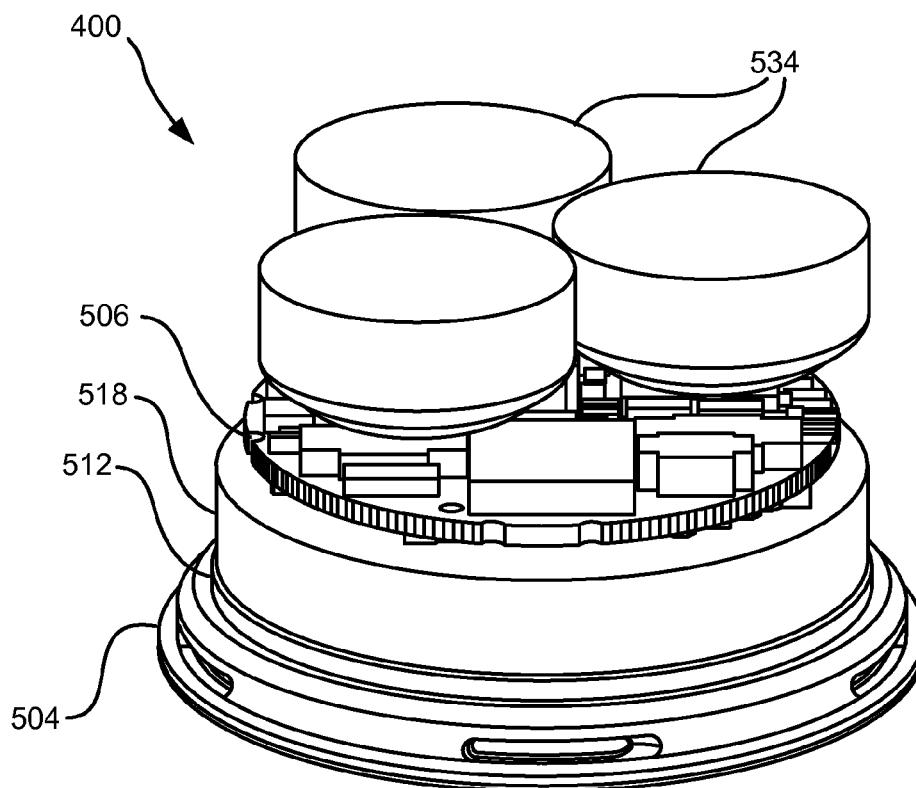


Fig. 5B

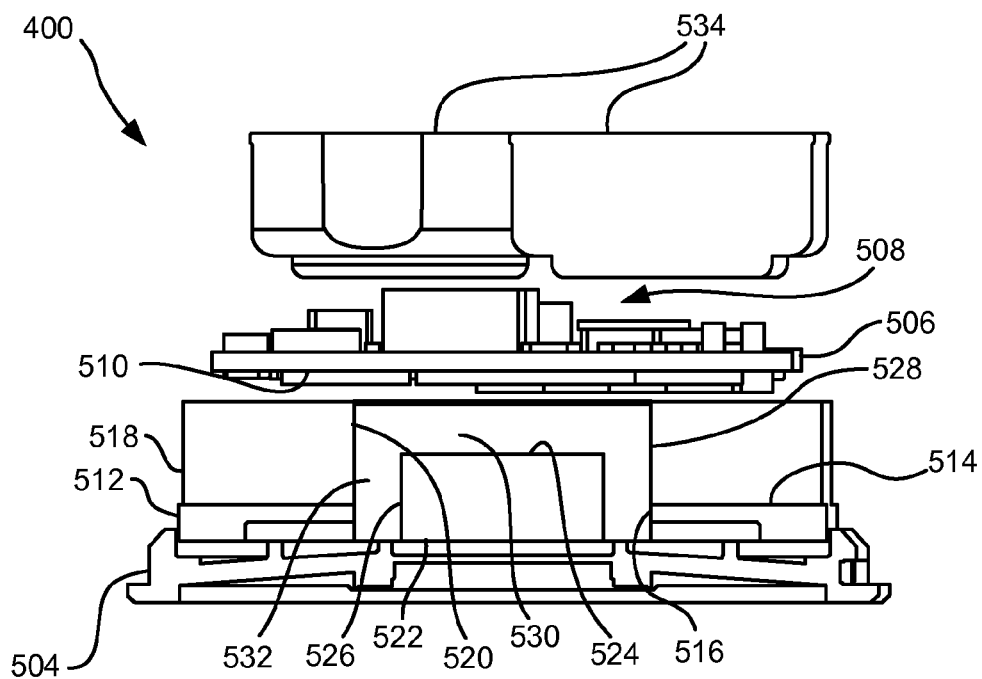


Fig. 5C

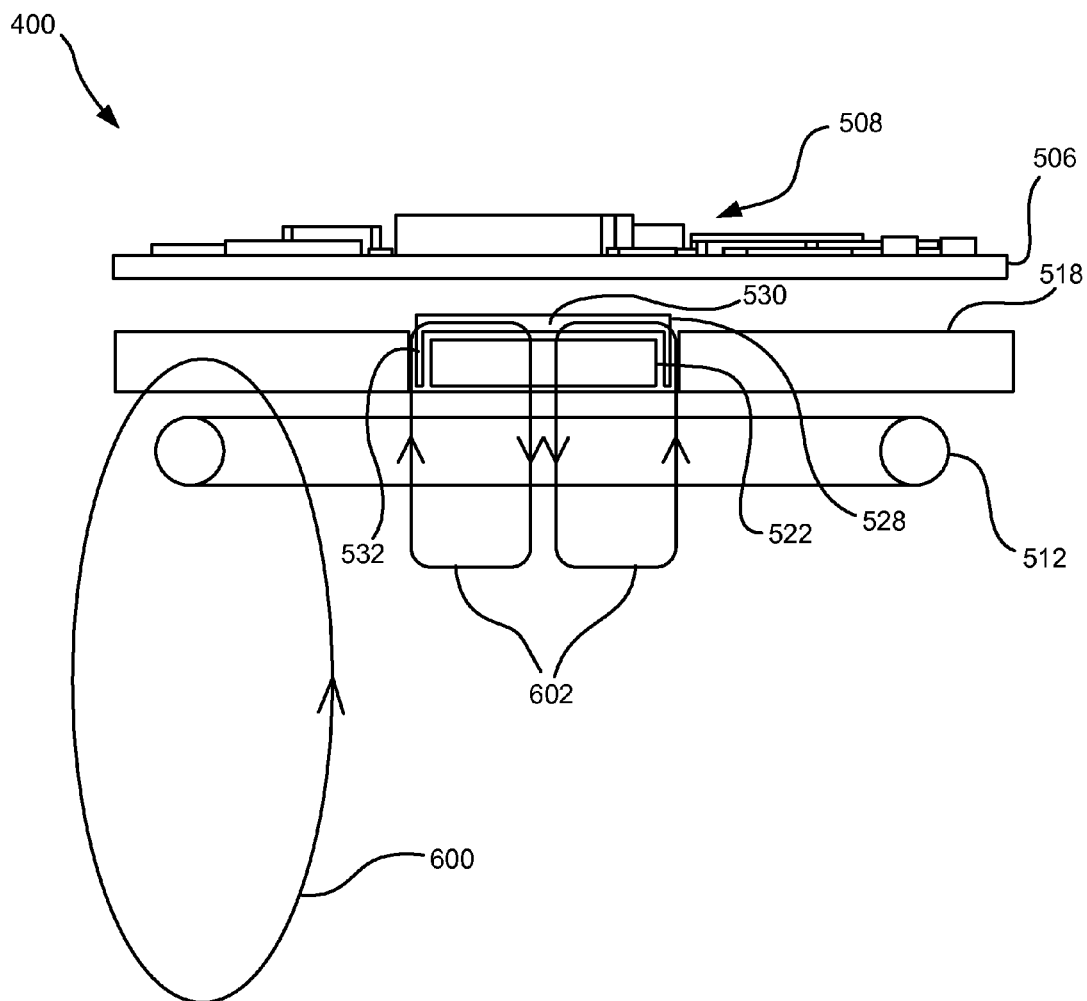


Fig. 6

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COCHLEAR IMPLANT SYSTEMS INCLUDING MAGNETIC FLUX REDIRECTION MEANS

RELATED APPLICATIONS

The present application is a continuation application of U.S. patent application Ser. No. 13/128,755, filed May 11, 2011, is now U.S. Pat. No. 8,897,883, which application is a U.S. National Stage Entry of PCT Application No. PCT/US09/64033, filed Nov. 11, 2009, which application claims priority to U.S. Provisional Patent Application No. 61/113,675, filed Nov. 12, 2008, U.S. Provisional Patent Application No. 61/113,708, filed Nov. 12, 2008, and U.S. Provisional Patent Application No. 61/139,567, filed Dec. 20, 2008. The contents of all of these applications are incorporated herein by reference in their respective entireties.

BACKGROUND INFORMATION

The sense of hearing in human beings involves the use of hair cells in the cochlea that convert or transduce audio signals into auditory nerve impulses. Hearing loss, which may be due to many different causes, is generally of two types: conductive and sensorineural. Conductive hearing loss occurs when the normal mechanical pathways for sound to reach the hair cells in the cochlea are impeded. These sound pathways may be impeded, for example, by damage to the auditory ossicles. Conductive hearing loss may often be helped by the use of conventional hearing aids that amplify sound so that audio signals reach the cochlea and the hair cells. Some types of conductive hearing loss may also be treated by surgical procedures.

Sensorineural hearing loss, on the other hand, is due to the absence or the destruction of the hair cells in the cochlea which are needed to transduce audio signals into auditory nerve impulses. Thus, many people who suffer from severe to profound sensorineural hearing loss are unable to derive any benefit from conventional hearing aid systems. To overcome sensorineural hearing loss, numerous cochlear implant systems, or cochlear prosthesis, have been developed. Cochlear implant systems bypass the hair cells in the cochlea by presenting electrical stimulation directly to the auditory nerve fibers. Direct stimulation of the auditory nerve fibers leads to the perception of sound in the brain and at least partial restoration of hearing function.

Cochlear implant systems typically include a cochlear stimulator that is implanted beneath the scalp of a patient. An external control assembly located external to the patient's scalp may be used by the patient to control and adjust various operational parameters of the implanted cochlear stimulator. An inductive link is commonly used to transmit telemetry signals from the external control assembly to the implanted cochlear stimulator. To this end, the external control assembly often includes an inductive coil that produces a telemetry signal by generating an electro-magnetic field that is picked up by a receiver on the implanted cochlear stimulator. The inductive coil may be housed in an external headpiece that is positioned on a patient's head to transmit the telemetry signal through the patient's scalp to the implanted receiver. The external control often includes a retention magnet for securing the headpiece to the patient's head so that the induction coil is properly positioned adjacent to the implanted receiver.

In a conventional cochlear implant system, electronic circuitry included within the external control assembly is not placed in relative close proximity to the induction coil and the retention magnet due to losses and interference caused by

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magnetic flux associated with the induction coil and the retention magnet. Hence, the electronic circuitry is typically housed within a behind-the-ear unit, for example, while the induction coil and the retention magnet are housed separately within a headpiece. Such a configuration is undesirable for many cochlear implant patients.

SUMMARY

Exemplary cochlear implant systems include a circuit board having electronic circuitry configured to generate one or more signals configured to direct electrical stimulation of one or more stimulation sites within a patient, an induction coil configured to transmit a telemetry signal by generating a telemetry magnetic field, and a telemetry flux guide positioned between the induction coil and the circuit board. The telemetry flux guide is configured to direct magnetic flux of the telemetry magnetic field away from the circuit board.

Exemplary cochlear implant systems include a circuit board having electronic circuitry configured to generate one or more signals configured to direct electrical stimulation of one or more stimulation sites within a patient, a retention magnet configured to produce a retention magnetic field for securing one or more components of the cochlear implant system to a head of said patient, and a retention flux guide positioned between the retention magnet and the circuit board. The retention flux guide is configured to direct magnetic flux of the retention magnetic field away from the circuit board.

Exemplary external headpieces for use in cochlear implant systems include a circuit board having electronic circuitry configured to generate one or more signals configured to direct electrical stimulation of one or more stimulation sites within a patient. The external headpieces further include an induction coil configured to transmit a telemetry signal by generating a telemetry magnetic field and a telemetry flux guide positioned between the induction coil and the circuit board. The telemetry flux guide is configured to direct magnetic flux of the telemetry magnetic field away from the circuit board.

BRIEF DESCRIPTION OF THE DRAWINGS

The accompanying drawings illustrate various embodiments of the principles described herein and are a part of the specification. The illustrated embodiments are merely examples and do not limit the scope of the disclosure.

FIG. 1A illustrates an exemplary cochlear implant system according to principles described herein.

FIG. 1B illustrates a portion of an exemplary cochlear implant system according to principles described herein.

FIG. 2 is a functional block diagram of an exemplary sound processor and implantable cochlear stimulator according to principles described herein.

FIG. 3 illustrates a schematic structure of the human cochlea highlighting elements according to principles described herein.

FIG. 4 illustrates an exemplary configuration of a cochlear implant system according to principles described herein.

FIG. 5A is an exploded perspective view of an exemplary external headpiece according to principles described herein.

FIG. 5B is a perspective view of a portion of an exemplary external headpiece according to principles described herein.

FIG. 5C is a cross-sectional side view of a portion of an exemplary external headpiece according to principles described herein.

FIG. 6 illustrates magnetic flux surrounding an induction coil and a retention magnet in an exemplary external headpiece according to principles described herein.

Throughout the drawings, identical reference numbers designate similar, but not necessarily identical, elements.

DETAILED DESCRIPTION

Cochlear implant systems including an external headpiece that houses a circuit board having electronic circuitry configured to generate one or more signals configured to control an operation of an implantable cochlear stimulator are described herein. The external headpiece further includes an induction coil configured to transmit a telemetry signal to the implantable cochlear stimulator by generating a telemetry magnetic field. The external headpiece may additionally include a telemetry flux guide positioned between the induction coil and the circuit board. The telemetry flux guide may be configured to direct magnetic flux of the telemetry magnetic field away from the circuit board.

In some examples, the external headpiece further includes a retention magnet configured to produce a retention magnetic field for securing the headpiece to a head of the patient. In this case, the external headpiece may also include a retention flux guide positioned between the retention magnet and the circuit board. The retention flux guide may be configured to direct magnetic flux of the retention magnetic field away from the circuit board.

In the following description, for purposes of explanation, numerous specific details are set forth in order to provide a thorough understanding of the present systems and methods. It will be apparent, however, to one skilled in the art that the present systems and methods may be practiced without these specific details. Reference in the specification to “one example” or “an example” means that a particular feature, structure, or characteristic described in connection with the example is included in at least one example. The appearance of the phrase “in one example” in various places in the specification are not necessarily all referring to the same example.

FIG. 1A illustrates an exemplary cochlear implant system 100. The cochlear implant system 100 of FIG. 1A includes a sound processor portion 102 and a cochlear stimulation portion 104. The sound processor portion 102 may include a sound processor 106, a microphone 108, and/or additional circuitry as best serves a particular application. The cochlear stimulation portion 104 may include an implantable cochlear stimulator 110, a number of electrodes 112 disposed on an electrode lead 114, and/or additional circuitry as best serves a particular application. The components within the sound processor portion 102 and the cochlear stimulation portion 104 will be described in more detail below.

The microphone 108 of FIG. 1A is configured to sense audio signals and convert the sensed signals to corresponding electrical signals. In some examples, the audio signal may include speech. The audio signal may additionally or alternatively include music, noise, and/or other sounds. The electrical signals are sent from the microphone 108 to the sound processor 106 via a communication link 116. Alternatively, the microphone 108 may be connected directly to, or integrated with, the sound processor 106. The sound processor 106 processes these converted audio signals in accordance with a selected sound processing strategy to generate appropriate stimulation parameters for controlling the implantable cochlear stimulator 110. These stimulation parameters may specify or define the polarity, magnitude, location (i.e., which electrode pair or electrode group receive the electrical stimulation), stimulation rate, timing (i.e., when the electrical

stimulation is to be applied to a particular electrode pair), spectral tilt, and/or any other characteristic of the electrical stimulation that is generated by the implantable cochlear stimulator 110.

The electrode lead 114 shown in FIG. 1A is configured to be inserted within a duct of a cochlea. As shown in FIG. 1A, the electrode lead 114 includes a multiplicity of electrodes 112, e.g., sixteen electrodes, spaced along its length. It will be understood, however, that any number of electrodes 112 may be disposed on the electrode lead 114. The electrode lead 114 may be substantially as shown and described in U.S. Pat. Nos. 4,819,647 or 6,218,753, each of which is incorporated herein by reference in its respective entirety. As will be described in more detail below, electronic circuitry within the implantable cochlear stimulator 110 is configured to generate and apply electrical stimulation to one or more stimulation sites within the cochlea via selected stimulation channels (i.e., pairs or groups of the individual electrodes 112) in accordance with a specified stimulation strategy defined by the sound processor 106.

In some examples, the sound processor 106 and the microphone 108 comprise an external portion of the cochlear implant system 100, and the implantable cochlear stimulator 110 and the electrode lead 114 comprise an implantable portion of the system 100 that is implanted within a patient's body. In alternative embodiments, one or more portions of the sound processor 106 are included within the implantable portion of the cochlear implant system 100.

The implantable cochlear stimulator 110 and the sound processor 106 may be communicatively coupled via a suitable data or communication link 118, such as a telemetry communication link, as will be described in more detail below. It will be understood that the data communication link 118 may include a bi-directional communication link and/or one or more dedicated uni-directional communication links. In some examples, the external and implantable portions of the cochlear implant system 100 may each include one or more inductive coils configured to transmit and receive power and/or control signals via the communication link 118. The control signals may include, for example, the magnitude and polarity of electrical stimulation representing a sensed audio signal. The external coil may also transmit power from the external portion to the implantable portion of the cochlear implant system 100. Power transmitted to the implantable portion may be used to operate the implantable portion.

FIG. 1B illustrates a portion of an exemplary cochlear implant system showing a communication link 118 comprising a telemetry communication link that may be used in accordance with the present systems and methods. As illustrated in FIG. 1B, an external portion of the cochlear implant system 100 may include an external induction coil 120 and an implantable portion of the cochlear implant system 100 may include an implantable induction coil 122. The external induction coil 120 may be communicatively coupled to the sound processor 106 and the implantable induction coil 122 may be communicatively coupled to the implantable cochlear stimulator 110.

The external induction coil 120 and the implantable induction coil 122 may include any suitable type of coil capable of generating and/or receiving an electro-magnetic field. For example, the external induction coil 120 and the implantable induction coil 122 may each include a metallic wire or tube wound in a coiled or otherwise looped configuration. An alternating current may be directed from the sound processor 106 through the external induction coil 120, thereby generating a magnetic field surrounding the external induction coil 120. The external induction coil 120 may be positioned near

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the implantable induction coil **122** such that the implantable induction coil **122** is positioned at least partially within the magnetic field generated by the external induction coil **120**. The magnetic field generated by the external induction coil **120** may cause an electric current to be generated in the internal induction coil **120**. The electric current generated in the internal induction coil **120** may be directed from the internal induction coil **120** to the implantable cochlear stimulator **110**. Accordingly, an electric current generated by the sound processor **106** may be transferred to the implantable cochlear stimulator **110** through the communication link **118** comprising the external induction coil **120** and the implantable induction coil **122**.

The communication link **118** may function as a telemetry link between the sound processor **106** and the implantable cochlear stimulator **110**. For example, the external induction coil **120** may transmit one or more telemetry signals to the implantable induction coil **122** by generating a telemetry magnetic field as electric current is passed through the external induction coil **120**. The telemetry magnetic field generated by the external induction coil **120** may produce an electric current in the implantable induction coil **122**, as described above. The current generated in the implantable induction coil **122** by the telemetry magnetic field generated by the external induction coil **120** may be used to transfer signals representative of data and/or other information to the implantable cochlear stimulator **110** and/or may be used to transfer power to the implantable cochlear stimulator **110**.

In some examples, the communication link **118** may be used to transmit telemetry signals from the implantable cochlear stimulator **110** to the sound processor **106**. For example, data acquired by the electrodes **112** and/or status indicators generated by the cochlear stimulator **112** may be transmitted to sound processor **106** via the communication link **118**. To this end, implantable induction coil **122** may transmit telemetry signals to the external induction coil **120** by generating a telemetry magnetic field. The implantable cochlear stimulator **110** may cause a current to flow through the implantable induction coil **122** to generate the telemetry magnetic field. The external induction coil **120** may be positioned at least partially within the telemetry magnetic field generated by the implantable induction coil **122**. The magnetic field may cause an electric current to be generated in the external induction coil **120**. The current generated in the external induction coil **120** may be used to transfer data and/or other signals to the sound processor **106**.

The communication link **118** may include more than one external induction coil **120** and/or more than one implantable induction coil **122**. For example, a first external induction coil and a first implantable induction coil may be used to transfer data and/or power from the sound processor **106** to the implantable cochlear stimulator **110**. A second external induction coil and a second implantable induction coil may be used to transfer data from the implantable cochlear stimulator **110** to the sound processor **106**.

FIG. 2 is a functional block diagram of an exemplary sound processor **106** and implantable cochlear stimulator **110**. The functions shown in FIG. 2 are merely representative of the many different functions that may be performed by the sound processor **106** and/or the implantable cochlear stimulator **110**.

As shown in FIG. 2, the microphone **108** senses an audio signal, such as speech or music, and converts the audio signal into one or more electrical signals. These signals are then amplified in audio front-end (AFE) circuitry **202**. The amplified audio signal is then converted to a digital signal by an analog-to-digital (A/D) converter **204**. The resulting digital

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signal is then subjected to automatic gain control using a suitable automatic gain control (AGC) function **206**.

After appropriate automatic gain control, the digital signal is then processed in one of a number of digital signal processing or analysis channels **208**. For example, the sound processor **106** may include, but is not limited to, sixteen analysis channels **208**. Each analysis channel **208** may respond to a different frequency band of the sensed audio signal due to a series of band pass filters **210**.

As shown in FIG. 2, each of the *m* analysis channels **208** may also include an energy detection stage (D1-Dm) **212**. Each energy detection stage **212** may include any combination of circuitry configured to detect the amount of energy contained within each of the *m* analysis channels **208**. For example, each energy detection stage **212** may include a rectification circuit followed by an integrator circuit.

After energy detection, the signals within each of the *m* analysis channels **208** are forwarded to a mapping stage **214**. The mapping stage **214** is configured to map the signals in each of the *m* analysis channels **208** to one or more of *M* stimulation channels **218**. In other words, the information contained in the *m* analysis channels **208** is used to define the electrical stimulation pulses that are applied to the patient by the implantable cochlear stimulator **110** via the *M* stimulation channels **218**. As mentioned previously, pairs or groups of individual electrodes **112** may make up the *M* stimulation channels **218**.

In some examples, the mapped signals are serialized by a multiplexer **216** and transmitted to the implantable cochlear stimulator **110**. The implantable cochlear stimulator **110** may then apply electrical stimulation via one or more of the *M* stimulation channels **218** to one or more stimulation sites within the duct of the patient's cochlea. As used herein, the term "stimulation site" will be used to refer to a target area or location to which the electrical stimulation is applied. For example, a stimulation site may refer to any location within a region of auditory nerve tissue (e.g., auditory nerve tissue **306** shown in FIG. 3).

FIG. 3 illustrates a schematic structure of the human cochlea **300**. As shown in FIG. 3, the cochlea **300** is in the shape of a spiral beginning at a base **302** and ending at an apex **304**. Within the cochlea **300** resides auditory nerve tissue **306**, which is denoted by Xs in FIG. 3. The auditory nerve tissue **306** is organized within the cochlea **300** in a tonotopic manner. Low frequencies are encoded at the apex **304** of the cochlea **300** while high frequencies are encoded at the base **302**. Hence, each location along the length of the cochlea **300** corresponds to a different perceived frequency. A cochlear prosthesis may therefore be implanted within a patient with sensorineural hearing loss and configured to apply electrical stimulation to different locations within the cochlea **300** to provide the sensation of hearing. For example, electrode lead **114** may be disposed within the cochlea **300** such that electrodes **112** contact auditory nerve tissue **306** within the cochlea **300**. Electrical stimulation may be applied by the electrodes **112** to the auditory nerve tissue **306**.

FIG. 4 illustrates an exemplary configuration of cochlear implant system **100** that may be used to apply electrical stimulation one or more stimulation sites within the cochlea **300**. As shown in FIG. 4, the external portion of the cochlear implant system **100** may include an external headpiece **400** configured to be worn on an exterior of a head **402** of the patient. The external headpiece **400** may include various components of the sound processor portion **102**, including the external induction coil **122** (not shown), as will be described in greater detail below. The external headpiece **400** may additionally include electronic circuitry, such as circuitry com-

prising at least a portion of the sound processor **106**. The external headpiece **400** may be electrically connected, either directly or indirectly, to a microphone **108** (not shown) positioned in or near the patient's ear via a communication line **404**. The headpiece **400** may additionally include a retention magnet to position and maintain the headpiece **400** in a proper orientation on the head **402**, as will be described in greater detail below.

As shown in FIG. 4, an implantable cochlear stimulator **110** may be disposed underneath the skin **406** of the patient. A lead **114** with a plurality of electrodes **112** disposed on a distal portion thereof may be coupled to the implantable cochlear stimulator **110** and positioned such that the electrodes **112** are disposed within the cochlea **300**.

In some examples, the implantable cochlear stimulator **110** may include a receiver **408** configured to facilitate communication with the external headpiece **400**. The receiver **408** may include the implantable induction coil **122** (not shown) described above.

The external induction coil **120** in the external headpiece **400** and the implantable induction coil **122** in the receiver **408** may form communication link **118**. As described above, data and/or power may be transmitted between the sound processor portion **102** and the cochlear stimulation portion **104** via the communication link **118**. For example, the external induction coil **120** in the external headpiece **400** may transmit a telemetry signal across the skin **406** to the implantable induction coil **122** in the receiver **408**. Additionally or alternatively, the implantable induction coil **122** in the receiver **408** may transmit a telemetry signal across the skin **406** to the external induction coil **120** in the external headpiece **400**.

FIGS. 5A-5C illustrate an exemplary external headpiece **400** that may be used in accordance with present systems and methods. The components shown in FIGS. 5A-5C are merely illustrative of the many different components that may be included within headpiece **400**. Additional or alternative components may be included within headpiece **400** as may serve a particular application.

FIG. 5A is an exploded perspective view of the exemplary external headpiece **400** showing various components of the external headpiece **400**. FIG. 5B is a perspective view of the exemplary external headpiece **400** shown without a headpiece cover. FIG. 5C is cross-sectional side view of the exemplary external headpiece **400** shown without a headpiece cover. As shown in FIGS. 5A-5C, the external headpiece **400** may include a headpiece cover **500** in which a headpiece cavity **502** is defined. The external headpiece **400** may additionally include a headpiece base **504** that may be attached to the headpiece cover **500**. Components in the external headpiece **400** may be housed in the headpiece cavity **502** such that they are substantially surrounded by headpiece cover **500** and the headpiece base **504**.

The external headpiece **400** may include a circuit board **506** (e.g., a printed circuit board) having electronic circuitry **508** disposed thereon. The electronic circuitry **508** may be disposed on any suitable portions of the circuit board **506**. A bottom surface **510** of the circuit board **506** may face generally towards the headpiece base **504**. The electronic circuitry **508** may include the sound processor **106** or at least a portion of the sound processor **106**. The electronic circuitry **508** may be configured to direct the implantable cochlear stimulator **110** to generate and apply electrical stimulation to one or more stimulation sites within the cochlea **300** of a patient by transmitting control parameters (including, but not limited to, stimulation parameters) to the implantable cochlear stimulator **110** via communications link **118**. The electronic circuitry **508** may additionally or alternatively be configured to trans-

mit power to the implantable cochlear stimulator **110** and may be configured to receive data from the cochlear stimulator **110**.

The external headpiece **400** may further include an induction coil **512** disposed below the bottom surface **510** of the circuit board **506**. The induction coil **512** may include a metallic wire or tube wound in a coiled configuration. In some examples, the induction coil **512** may include a coiled wire arranged in a generally disc-shaped and/or annular-shaped holder. It will be recognized that the induction coil **512** may have any suitable size and shape as may serve a particular application.

The induction coil **512** may have a top surface **514** and an interior radial surface **516**, as illustrated in FIG. 5A. The induction coil **512** may be seated in the headpiece base **504**. Accordingly, the induction coil **512** may be in close proximity to the head **402** of the patient when the headpiece base **504** is adjacent to the head **402**.

In some examples, the external headpiece **400** may additionally include a telemetry flux guide **518** positioned or disposed between the circuit board **506** and the induction coil **512**. The telemetry flux guide **518** may have a generally annular shape with an inner radial surface **520** defining an aperture extending through a central portion of the telemetry flux guide **518**. The telemetry flux guide may be adjacent to the bottom surface **510** of the circuit board **506** and the top surface **514** of the induction coil **512**.

The telemetry flux guide **518** may include any material suitable for directing magnetic flux away from the circuit board **506**. For example, the telemetry flux guide **518** may include a material having a relatively high resistivity that provides a low reluctance path for magnetic flux of the telemetry magnetic field. Additionally, the telemetry flux guide **518** may include a powdered material, such as a powdered metallic material having a relatively small particle size, in order to prevent the generation of eddy current in the telemetry flux guide **518**. For example, eddy currents might be generated in a solid conductive material (as opposed to a powdered conductive material) in the presence of the telemetry magnetic field since the telemetry magnetic field is a changing magnetic field generated by an alternating current passing through the induction coil **512**.

The powdered material in telemetry flux guide **518** may be held together using any suitable material, such as a polymer material. In some examples, the powdered metallic material may include iron and/or other ferrite materials. Additionally, the telemetry flux guide **518** may be suitable for frequencies of telemetry signals generated and/or received by the induction coil **512**, such as, for example, an approximately 49 MHz telemetry signal and/or an approximately 10.7 MHz telemetry signal. A telemetry flux guide **518** including a material having a relative permeability (i.e., the ratio of the permeability of the alloy to the permeability of free-space) of approximately 9 may be suitable for a frequency range that includes 49 MHz and 10.7 MHz telemetry signals. However, it will be recognized that the telemetry flux guide **518** may have any other suitable relative permeability value as may serve a particular application. Additionally or alternatively, telemetry flux guide **518** may have a relatively high resistivity and a relatively small particle size in order to facilitate redirection of magnetic flux while minimizing the generation of eddy currents in the telemetry flux guide **518**.

The telemetry flux guide **518** may be positioned and configured to direct magnetic flux of the magnetic field generated by the induction coil **512** away from the circuit board **506**, as will be described in greater detail below. For example, a telemetry magnetic field may generated by the induction coil

512 to transmit a telemetry signal. Magnetic flux of the telemetry magnetic field may be directed away from the circuit board **506** by the telemetry flux guide **518**, thereby protecting the electronic circuitry **508** on the circuit board **506** from the telemetry magnetic field. By directing the magnetic flux in the telemetry magnetic field away from the circuit board **506**, energy losses from the induction coil **512** to the electronic circuitry **508** via the telemetry magnetic field may be minimized, thereby extending the life of batteries used to provide power to one or more components of the cochlear implant system **100**.

In some examples, the external headpiece **400** may additionally or alternatively include a retention magnet **522** disposed between the circuit board **506** and the headpiece base **504**. The retention magnet **522** may have a top surface **524** generally facing the bottom surface **510** of the circuit board **506**. The retention magnet **522** may additionally have an outer radial surface **526**. In some embodiments, the retention magnet **522** may be positioned in the external headpiece **400** such that the retention magnet **522** is at least partially surrounded by the induction coil **512** and/or the telemetry flux guide **518**. Accordingly, the outer radial surface **526** of the retention magnet **522** may generally face the inner radial surface **516** of the induction coil **512** and/or the inner radial surface **520** of the telemetry flux guide **518**. For example, the retention magnet **522** may be positioned in an aperture defined by the inner radial surface **520** extending through the telemetry flux guide **518**.

The retention magnet **522** may be configured to produce a retention magnetic field for securing one or more components of a cochlear implant system **100** to a head **402** of a patient. For example, the retention magnet **522** may be disposed adjacent to the headpiece base **504** such that the retention magnet **522** is in close proximity to the head **402** of the patient when the headpiece base **504** is adjacent to the head **402**. A portion of the cochlear stimulation portion **104** of the cochlear implant system **100**, such as the receiver **408** shown in FIG. 4, may similarly include a magnet configured to magnetically couple with the retention magnet **522**. Accordingly, when the headpiece base **504** is positioned adjacent to the head **402** of the patient near the receiver **408**, the retention magnet **522** may be magnetically coupled to the magnet of the cochlear stimulation portion **104**, thereby securing and/or orienting the external headpiece **400** on the head **402**.

The external headpiece **400** may additionally or alternatively include a retention flux guide **528** positioned between the circuit board **506** and the retention magnet **522**. The retention flux guide **528** may at least partially surround the retention magnet **522**. As illustrated in FIGS. 5A and 5C, a top wall **530** of the retention flux guide **528** may be disposed between and adjacent to the bottom surface **510** of the circuit board **506** and the top surface **524** of the retention magnet **522**. Additionally, a side wall **532** of the retention flux guide **528** may at least partially surround the outer radial surface **526** of the retention magnet **522**. The side wall **532** of the retention flux guide **528** may be adjacent to the outer radial surface **526** of the retention magnet **522**, the inner radial surface **516** of the induction coil **512**, and/or the inner radial surface **520** of the telemetry flux guide **518**.

The retention flux guide **528** may include any material suitable for redirecting magnetic flux associated with a magnetic field produced by the retention magnet **522**. For example, the retention flux guide **528** may include a material having a relatively high permeability. In some examples, the retention flux guide **528** may include a metallic material, such as a mu-metal alloy comprising nickel and iron. A relatively high permeability mu-metal alloy may have a relative perme-

ability between approximately 60,000 and 300,000. For example, a mu-metal alloy may have a relative permeability of approximately 100,000. A high-permeability mu-metal alloy may include any suitable ratio of nickel and iron, such as, for example, a ratio of approximately 80% nickel and 20% iron. It will be recognized that the retention flux guide **528** may alternatively include any suitable material having any suitable relative permeability.

The retention flux guide **528** may be configured to direct magnetic flux of a retention magnetic field surrounding the retention magnet **522** away from the circuit board **506** and/or away from the telemetry flux guide **518**. Accordingly, magnetic flux from the retention magnet **522** may be directed away from the circuit board **506**, thereby protecting the electronic circuitry **508** on the circuit board **506** from the retention magnetic field.

As mentioned, the retention flux guide **528** may also direct magnetic flux of the retention magnetic field away from the telemetry flux guide **518**, thereby preventing saturation of powdered metallic material in the telemetry flux guide **518** with magnetic flux from the retention magnet. Magnetic flux from the retention magnet **522** may significantly reduce the relative permeability of the powdered metallic material in the telemetry flux guide **518**, reducing the effectiveness of the telemetry flux guide **518** in directing magnetic flux from the induction coil **512** away from the circuit board **506**. Accordingly, the retention flux guide **528** may direct magnetic flux of the retention magnetic field away from the telemetry flux guide **518**, thereby preventing magnetic flux from saturating the telemetry flux guide **518**.

By directing magnetic flux away from the electronic circuitry **508** in the circuit board **506**, the telemetry flux guide **518** and/or the retention flux guide **528** may enable the induction coil **512** and/or the retention magnet **522** to be located within the external headpiece **400** in relatively close proximity to the circuit board **506**. Accordingly, the sound processor portion **102** of the cochlear implant system **100** may be made more compact by consolidating electronic and magnetic field emitting components within the headpiece as illustrated in FIGS. 5A-5C. This may increase the ease of use and comfort for a patient using the cochlear implant system **100** in comparison to conventional cochlear implant systems in which electronic circuitry is separated from the headpiece. For example, a consolidated assembly, such as that illustrated in FIGS. 5A-5C, may eliminate the need for a separate behind-the-ear assembly. Hence, the assembly illustrated in FIGS. 5A-5C may be referred to as a "one piece system headpiece".

In some embodiments, the cochlear stimulation portion **104** of a cochlear implant system **100** may additionally or alternatively include a retention flux guide and/or a telemetry flux guide for directing magnetic flux away from electronic components in the cochlear stimulation portion **104**. For example, a receiver **408** in the cochlear stimulation portion **104** may include an induction coil and/or a retention magnet, similar to the external headpiece **400** as described above. A retention flux guide and/or a telemetry flux guide may be included in the receiver **408** to redirect magnetic flux away from electronic circuitry that may be located in close proximity to the induction coil and/or the retention magnet.

Additionally, as illustrated in FIGS. 5B and 5C, the external headpiece **400** may include one or more batteries **534** to power the sound processor portion **102** and/or the cochlear stimulation portion **102** of the cochlear implant system **100**. Batteries **534** may be disposed within the headpiece cover cavity **502** of the headpiece cover **500** and may be located adjacent circuit board **506**. In some embodiments, batteries **534** may be located outside of the external headpiece **400**.

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FIG. 6 illustrates magnetic flux surrounding an induction coil 512 and a retention magnet 522 in an exemplary external headpiece 400 in accordance with the present systems and methods. As illustrated in FIG. 6, magnetic flux 600 may surround the induction coil 512. The magnetic flux 600 is represented as a flux path surrounding the induction coil 512. Additionally, magnetic flux 602 may pass through and surround retention magnet 522. The magnetic flux 602 is represented as flux paths surrounding and passing through the retention magnet 522. It will be recognized that additional flux paths other than those illustrated in FIG. 6 may be associated with the telemetry magnetic field surrounding the induction coil 512 and the retention magnetic field surrounding the retention magnet 522.

The telemetry flux guide 518 may provide a low reluctance path for the magnetic flux 600 surrounding the induction coil 512. As illustrated in FIG. 6, the path of the magnetic flux 600 may be directed through the telemetry flux guide 518 such that a path of the magnetic flux 600 between the induction coil 512 and the circuit board 506 may be shortened. The magnetic flux 600 of the telemetry magnetic flux field surrounding the induction coil 512 may therefore be redirected by the telemetry flux guide 518 such that the magnetic flux 600 is substantially prevented from reaching the circuit board 506, thereby reducing or eliminating magnetic flux passing through the electronic circuitry 508.

The retention flux guide 528 may provide a high permeability path for the magnetic flux 602 surrounding and passing through the retention magnet 522. As illustrated in FIG. 6, the path of the magnetic flux 602 may be directed through the retention flux guide 528 such that a path of the magnetic flux 602 passes generally through and/or along the top wall 530 and/or the side wall 532 of the retention flux guide 528. Accordingly, a path of the magnetic flux 602 between the induction coil 512 and the circuit board 506 may be shortened. Similarly, a path of the magnetic flux 602 between the retention magnet 522 and the telemetry flux guide 518 may be shortened. The magnetic flux 602 of the retention magnetic flux field surrounding and passing through the retention magnet 522 may therefore be redirected by the retention flux guide 528 such that the magnetic flux 602 is substantially prevented from reaching the circuit board 506 and/or the telemetry flux guide 518, thereby reducing or eliminating magnetic flux from the retention magnet passing through the electronic circuitry 508 and/or the telemetry flux guide 518.

The preceding description has been presented only to illustrate and describe embodiments of the invention. It is not intended to be exhaustive or to limit the invention to any precise form disclosed. Many modifications and variations are possible in light of the above teaching.

What is claimed is:

1. A cochlear implant system associated with a patient and comprising:

- a component external to the patient and that houses a circuit board comprising electronic circuitry that generates one or more signals;
- an induction coil that transmits the one or more signals by generating a telemetry magnetic field; and
- a telemetry flux guide positioned between and in direct physical contact with a top surface of the induction coil and a bottom surface of the circuit board.

2. The cochlear implant system of claim 1, wherein the component further comprises a retention magnet that produces a retention magnetic field for securing one or more components of the cochlear implant system to a head of the patient.

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3. The cochlear implant system of claim 2, wherein the retention magnet is positioned in an aperture extending through the telemetry flux guide.

4. The cochlear implant system of claim 2, wherein the component further comprises a retention flux guide positioned between the retention magnet and the circuit board, wherein the retention flux guide directs magnetic flux of the retention magnetic field away from the circuit board.

5. The cochlear implant system of claim 4, wherein at least a portion of the retention flux guide is positioned between the retention magnet and the telemetry flux guide.

6. The cochlear implant system of claim 4, wherein the retention flux guide comprises a metal having a comparatively high relative permeability.

7. The cochlear implant system of claim 1, wherein the telemetry flux guide has an annular shape.

8. The cochlear implant system of claim 1, wherein the telemetry flux guide comprises a material having a relatively high resistivity that provides a low reluctance path for a magnetic flux of the telemetry magnetic field.

9. The cochlear implant system of claim 1, wherein the telemetry flux guide comprises a powdered metallic material.

10. The cochlear implant system of claim 9, wherein the powdered metallic material comprises a ferrite material.

11. The cochlear implant system of claim 1, wherein the component comprises an external headpiece configured to be secured to an exterior of a head of the patient.

12. The cochlear implant system of claim 1, wherein the one or more signals include one or more stimulation parameters configured to direct an implantable cochlear stimulator to apply electrical stimulation to one or more stimulation sites within a patient.

13. The cochlear implant system of claim 1, wherein the telemetry flux guide directs magnetic flux of the telemetry magnetic field away from the circuit board.

14. The cochlear implant system of claim 1, wherein the telemetry flux guide minimizes energy losses from the induction coil to the electronic circuitry via the telemetry magnetic field.

15. A cochlear implant system associated with a patient and comprising:

- a component external to the patient and that houses a circuit board comprising electronic circuitry that generates one or more signals;
- an induction coil that transmits the one or more signals by generating a telemetry magnetic field;
- a telemetry flux guide positioned between and in direct physical contact with a top surface of the induction coil and a bottom surface of the circuit board;
- a retention magnet that produces a retention magnetic field for securing one or more components of the cochlear implant system to a head of a patient; and
- a retention flux guide positioned between the retention magnet and the circuit board.

16. The cochlear implant system of claim 15, wherein the retention flux guide directs magnetic flux of the retention magnetic field away from the circuit board, and wherein the retention magnet and the retention flux guide are positioned within an aperture extending through the telemetry flux guide.

17. A cochlear implant system comprising:

- an external headpiece configured to be secured to an exterior of a head of a patient and that houses:
 - a circuit board comprising electronic circuitry that generates a telemetry signal,
 - a first induction coil that transmits the telemetry signal by generating a telemetry magnetic field, and

a telemetry flux guide positioned between and in direct physical contact with a top surface of the first induction coil and a bottom surface of the circuit board; and an implantable cochlear stimulator implanted within the patient and that includes a second induction coil that receives the telemetry signal. 5

18. The cochlear implant system of claim **17**, wherein the telemetry flux guide directs magnetic flux of the telemetry magnetic field away from the circuit board.

19. The cochlear implant system of claim **17**, further comprising: 10

a lead electrically connected to the implantable cochlear stimulator and comprising a plurality of electrodes in communication with one or more stimulation sites within a cochlea of the patient; 15

wherein the telemetry signal directs the implantable cochlear stimulator to generate and apply electrical stimulation to the one or more stimulation sites via the plurality of electrodes.

20. The cochlear implant system of claim **17**, wherein the external headpiece further comprises: 20

a retention magnet that produces a retention magnetic field for securing one or more components of the cochlear implant system to the head of the patient; and

a retention flux guide positioned between the retention magnet and the circuit board; 25

wherein the retention flux guide directs magnetic flux of the retention magnetic field away from the circuit board.

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